Designing a Radioimmunometric Assay Kit for Prostate-Specific Antigen Measurement Using Polystyrene Tubes Coated By Immunochemical Method

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ABSTRACT

Background and Objective: Prostate specific antigen (PSA) is considered as one of the most reliable biomarkers of cancer and other known prostate diseases. In the present study, solid phase sandwich immunoradiometric assay was used to measure the amount of PSA. In this type of measurement, a pair of anti-PSA antibodies on the solid phase and labeled with Iodine-125, participate in forming a complex with two different epitopes of PSA.

Methods: Variables such as irradiation level, modification of polymer surfaces by alcohol washing, different concentrations and volumes of antibody, incubation temperature and drying conditions that influence the direct coating process were optimized. Finally, the stability, accuracy and precision of the laboratory kit were evaluated by comparison with a foreign kit.

Results: According to the obtained results, preliminary preparations such as irradiation, tube washing and specific temperature conditions are not required during the coating process. Drying by lyophilization method does not affect the quality of coating. Antibody concentration of 2.5 μg/ml and coating volume of 800 μl were determined as the optimum conditions for coating, which had good stability within a year. Alignment of results obtained from the domestic and foreign kits for accuracy of 30 samples from patients was confirmed by T-test (sig 2-tailed = 0.993 and 95% confidence interval). The short-term and long-term precision for three control ranges (low, medium, high) were less than 0.25 and 0.33 of allowable total error (TEa = 10%), respectively.

Conclusion: The produced domestic kit has acceptable precision according to the CLIA criteria.

Keywords: Biological testing, Radioimmunometric assay, monoclonal antibody, prostate specific antigen, prostate disease.

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INTRODUCTION
Prostate cancer is the sixth most common cancer in the world and the third most common type of cancer in men. Therefore, early diagnosis prior to progression and metastasis to other parts of the body is of great importance for prevention and patients’ follow-up. Prostate-specific antigen (PSA) is a 26-33 kDa single-chain glycoprotein and serine protease belonging to kallikrein family, which is secreted by the prostate (1). In blood, PSA molecule is either in free form or bound to serum protein, mainly to α-1-antichymotrypsin. The ratio of these two forms varies depending on the type of disease, and is a good indicator of the type of prostate disease (2,3). Thus, the amount of this antigen is measured as an effective marker in prostate disease screening tests and for timely diagnosis of prostate diseases. The PSA measurement prior to digital rectal examination can be also effective (4-6). The PSA level is measured as a tumor marker in immunological methods using monoclonal antibodies. These methods can detect the marker based on physical and biological features of the antigen-antibody complex (7,8). The Sandwich immunoradiometric assay was used in this study to measure PSA levels. In this type of measurement, a pair of anti-PSA specific antibodies on the solid phase and labeled with Iodine-125, participate with two different epitopes of PSA in forming a complex (9). Monoclonal antibody-coated solid phase is a key component of the immunoradiometric methods. Polymer beads, latex particles and polymer tubes are used as solid phase systems for coating with antibodies. The Iranian polystyrene polymer tubes were used in this study, due to simplicity of its application in the IRMA kit and finally the results of quality control using real samples and control serums for PSA analysis are discussed and compared with a valid foreign kit (Immunotech) with tubes coated via the indirect method and according to Clinical Laboratory Improvement Amendments (CLIA) criteria (13).

MATERIAL AND METHODS
Gamma counter (GammaTech co., model 600 B), fraction collector (Pharmacia Biotech), peristaltic pumps (Pharmacia LKB pump), Anti-PSA specific monoclonal antibody for coating (1.05 mg/ml, Medix Biochemica Co.) and Iranian polystyrene tubes (Kariz Mehr Co.) were purchased. Standard PSA concentrations (0,1,3,10,30,100 ng/ml), control serum (prepared at the nuclear biomolecule laboratory) and a pair of monoclonal antibodies labeled with iodine-125 (prepared at the labeling laboratory of Nuclear Science and Technology Research Institute) were used. The serum samples were obtained from male volunteers working in the laboratory of Yousef Abad and the Nuclear Science and Technology Research Institute. Sodium dihydrogen phosphate, disodium hydrogen phosphate, sodium azide, and Tris were purchased from Merck Co. Citric acid, sodium citrate, bovine serum albumin (BSA), sucrose, sodium azide, and Triton X100 were purchased from Sigma Co.

1. Direct coating of Iranian polystyrene tubes
Anti-PSA monoclonal antibody for coating with three specific concentrations (1, 2.5, 5 μg/ml) was prepared in coating buffer [(0.1M phosphate buffer containing 0.5% sodium azide (pH=7.4)]. Then, sufficient amounts of the antibody were added to the polystyrene tubes. After being at room temperature for 24 hours, the tubes were emptied and replaced with blocking buffer [0.05M tris, 0.02M citric acid, 0.04M sodium citrate, 1% BSA, 1% sucrose and 0.1% sodium azide (pH=7.4)]. The tubes were placed at room temperature for 24 hours. The tubes were emptied and kept in a refrigerator for necessary testing.
2. Analysis of IRMA kit for measurement of total PSA concentration A certain amount of sample (blood serum of males or control serum) or standards (prepared in the laboratory with concentrations of 0,1,3,10,30,100 ng/ml) with an appropriate volume of the labeled antibody [(a pair of monoclonal antibodies labeled with iodine-125 using the chloramine-T method (4)] were exposed to each other in the coated tubes for 2 hours. The tube were emptied and washed twice with 2 ml of washing solution (containing 0.1% Triton - X100), to remove debris and unabsorbed substances. The level of binding radioactivity was measured by the Gamma counter. Total PSA concentration in the sample is directly correlated with the amount of radioactivity. It should be noted that the control samples (C1, C2), standards and antibodies labeled with iodine-125 were prepared in the laboratory. The range of serum concentration of controls and standards was determined and controlled by the foreign kit.

3. Investigation of factors affecting the coating

Before coating, the amount of irradiation and alcohol-washing conditions were investigated for preliminary preparation. Different concentrations and volumes of the antibody were used for coating the tubes. The calibration curve was plotted using the standards, and the control samples were analyzed by comparison with the foreign kit (Immunotech). The incubation temperature was 25°C. After coating at optimal conditions, the tubes were dried using a vacuum drying system and lyophilization. After optimization of conditions, the stability, accuracy and precision of the kit were evaluated. All experiments were done in triplicate.

RESULTS

1. Investigation of factors affecting the coating

1.1 Effect of irradiation on tubes’ coatings

Before coating and for preliminary preparation, different doses of gamma-ray (10, 25 and 50 kGy) were irradiated. Then, coating was done using the direct method (5 μg/ml of antibody with coating volume of 800 μl per tube). The results of tubes’ analysis show that irradiation does not affect the results of the analysis (Table 1).

1.2 Effect of temperature and washing the tubes with alcohol Before coating and for preliminary preparation, the tubes were washed with alcohol and then coated with 5 μg/ml antibody and 800μl of coating buffer with different temperature conditions (room temperature and incubation at 25°C). It seems that incubation and washing with alcohol did not affect the coating process compared to normal conditions (room temperature, without washing) (Table 2).

1.3 Effect of antibody’s concentration and coating volume

Different concentrations and volumes of the antibody were used for coating the tubes (20 repetitions). The calibration curve was plotted using the standards of the foreign kit and the standards prepared at the laboratory, and the concentration of control samples were analyzed. The calibration curve for the domestic kit with optimal concentration and volume of antibody was compared using the foreign and domestic kits’ standards (Figure 1). To evaluate the accuracy of the data, the concentration of control samples was determined by the foreign kit (three repetitions). The calibration curve was plotted for each time of coating, and the concentration of controls was analyzed using the coated tubes (three repetitions). The average of results at different conditions was compared with the foreign kit [coefficient of variation (CV) <6%] (Figures 2 and 3). Based on the proper calibration curve (without Hook effect), low non-specific binding (less than 200 count/min) and comparison of C1 and C2 concentrations’ analysis using the domestic and foreign kits, 2.5 μg/ml of antibody and volume of 800 μl were found as the optimal conditions for coating. Stability of the coated tubes and quality control of the kit were investigated.

1.4 Effect of drying system for coated tubes

After passive coating at optimal conditions, the tubes were vacuum dried (30 minutes) and lyophilized (overnight). Comparison of mean concentrations of C1 and C2 showed that lyophilization did not affect the coating quality. However, the concentration of C2 obtained under vacuum drying was less than acceptable range. The stability of the kit prepared using lyophilization will be discussed in the next section.
Table 1 - Effect of irradiation on the analysis of coated tubes

<table>
<thead>
<tr>
<th>Dose (kGy)</th>
<th>Percentage of maximum binding/total count ratio</th>
<th>Concentration of sample C1 (ng/ml)</th>
<th>Concentration of sample C2 (ng/ml)</th>
</tr>
</thead>
<tbody>
<tr>
<td>0</td>
<td>39</td>
<td>5.58</td>
<td>17.09</td>
</tr>
<tr>
<td>10</td>
<td>32</td>
<td>5.52</td>
<td>16.89</td>
</tr>
<tr>
<td>25</td>
<td>31</td>
<td>5.50</td>
<td>15.10</td>
</tr>
<tr>
<td>50</td>
<td>34</td>
<td>5.50</td>
<td>16.15</td>
</tr>
</tbody>
</table>

Table 2- Effect of temperature and alcohol washing on the coating process

<table>
<thead>
<tr>
<th>Coating conditions</th>
<th>Percentage of maximum binding/total count ratio</th>
<th>Concentration of sample C1 (ng/ml)</th>
<th>Concentration of sample C2 (ng/ml)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Alcohol washing and room temperature</td>
<td>20</td>
<td>5.0</td>
<td>24.5</td>
</tr>
<tr>
<td>Alcohol washing and 25°C</td>
<td>19</td>
<td>4.9</td>
<td>23.6</td>
</tr>
<tr>
<td>No washing and room temperature</td>
<td>30</td>
<td>5.50</td>
<td>24.6</td>
</tr>
<tr>
<td>No washing and 25°C</td>
<td>26</td>
<td>4.50</td>
<td>20.5</td>
</tr>
</tbody>
</table>

Figure 1- Comparison of the calibration curves of the immunometric kit for measurement of PSA using the domestic and foreign kits' standards

Figure 2- Comparison of C1 concentrations in the domestic kit and the foreign kit using different antibody concentrations (1, 2.5 and 5 μg/ml) and coating volumes (400, 800, 1000 μg/ml)
Figure 3 - Comparison of C2 concentrations in the domestic kit and the foreign kit using different antibody concentrations (1, 2.5 and 5 μg/ml) and coating volumes (400, 800, 1000 μg/ml)

![Comparison of C2 concentrations](image)

Table 3 - Effect of drying condition on concentration of the control samples

<table>
<thead>
<tr>
<th>Drying condition</th>
<th>Concentration of C2 (4-8 ng/ml)</th>
<th>Concentration of C2 (18-27 ng/ml)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Without drying</td>
<td>5.3</td>
<td>19.2</td>
</tr>
<tr>
<td>Vacuum drying</td>
<td>5.5</td>
<td>14.5</td>
</tr>
<tr>
<td>Lyophilization</td>
<td>5.7</td>
<td>20.8</td>
</tr>
</tbody>
</table>

Figure 4 - Stability of the tubes over time

![Stability of the tubes](image)

Figure 5 - Comparison of linear regression analysis of real samples using the reference (comparative method) and domestic (test method) kits

![Linear Regression](image)
2. Stability of the coated tubes
In order to investigate the stability of coated tubes (at optimum conditions), the concentration of controls was measured at five different time intervals (Figure 4). The results show that the coated tubes had good stability for one year.

3. Quality control of IRMA kit containing coated tubes for analysis of total PSA concentration

3.1 Accuracy of the kit: In order to investigate the accuracy of the produced kit, 30 real samples were analyzed simultaneously using the foreign (Immunotech) and domestic kits. Linear regression analysis (Figure 5), T-test (to calculate components of regression), correlation coefficient ($R^2 = 0.993$), mean difference (bias=0.1) and total error ($TE_{cal}=1.6$) were studied. Alignment of results of the two kits was investigated according to the results obtained from the T-test.

Based on the paired independent t-Test (with equal variances in the results of the domestic and reference kits), Sig (2-tailed) 0.933 was achieved, which is much larger than 5% (95% confidence interval). Thus, the alignment of the results of both kits was confirmed.

3.2 The precision of the kit
In order to estimate the imprecision of the kit, test–retest reliability was analyzed for three control ranges [low (C1), medium (C2), high (C3)] with 20 repetitions in three runs. The means, standard deviation ($SD$) and CV (%) were calculated (Table 4). The SD of less than 0.25 of the allowable total error ($TE_{a}=10\%$) was obtained within a run ($Sw$-run). The SD of less than 0.33 of the $TE_{a}$ was achieved for long-term imprecision of overall standard deviation ($ST$ total). Short-term and long-term imprecisions were calculated according to the CLIA criteria. The precision of the PSA diagnostic kit was acceptable.

<table>
<thead>
<tr>
<th>Table 4- Precision of the total PSA diagnostic kit</th>
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</thead>
<tbody>
<tr>
<td>C1(ng/ml)</td>
</tr>
<tr>
<td>---</td>
</tr>
<tr>
<td>1</td>
</tr>
<tr>
<td>Means ( 20 repeats)</td>
</tr>
<tr>
<td>SDw-run*</td>
</tr>
<tr>
<td>CV%</td>
</tr>
<tr>
<td>(Within a run)</td>
</tr>
<tr>
<td>Total mean</td>
</tr>
<tr>
<td>SD- total*</td>
</tr>
<tr>
<td>Total CV%</td>
</tr>
<tr>
<td>(Between runs)</td>
</tr>
</tbody>
</table>

**DISCUSSION**

Normally, proteins are irreversibly adsorbed onto polymer or plastic surfaces. Higher molecular weight of protein is accompanied with a stronger adsorption. Antibodies are a group of proteins (immunoglobulins) that well exhibit this property. The irreversible adsorption onto plastic surface is called the coating phase. The coated tubes are the polymer tubes that antibodies are absorbed onto their internal surfaces. The protein absorption onto polymer depends on electrical charge of the protein and their hydrophobic interactions. First, a monomolecular antibody is formed on the hydrophobic plastic surface.

The nature of the binding mechanism is not clear, but the factors such as concentration, pH, ionic strength, time, temperature and viscosity are effective on the properties of the coated surfaces. The proteins will have their best coating at a specific pH close to their isoelectric point. Molarity of buffer is another effective factor. Antibody absorption level is inversely correlated with the concentration of buffer’s salts. The interaction conditions are optimized in the coating phases according to the kit’s assessment criteria. It is difficult to control the conditions in passive method of coating. Thus, covalent coupling between the protein and the plastic surface is recommended. In some cases, reactive groups such as carboxyl or amine are placed onto surfaces using chemical modification. However, the passive method of coating is practically easier and more cost-effective for manufacturers.

In this study, different conditions affecting the coating process were investigated to achieve coating technology for Iranian polymer tubes using a monoclonal antibody (passive method). Three specific concentrations of anti-PSA monoclonal antibody were coated on polystyrene tubes. The influencing factors such as irradiation, washing, temperature,
concentration and volume of the antibody were investigated. Each factor was compared within the desired range with regard to the kit’s analysis. The results showed that the factors such as irradiation and washing do not affect the quality of suitable site for coating onto the tubes’ polymer surface. However, the concentration and volume of the antibody affect the interaction between pair of antibodies. The impact of different concentrations and volumes of antibody for coating was analyzed by plotting calibration curve for concentrations of the control samples. Optimal coating conditions were determined with respect to the appropriate calibration curve (without Hook effect), low non-specific binding and comparison of control samples’ concentration analysis. Then, the stability of coated tubes and quality control of the kit were evaluated. Two methods of vacuum drying and lyophilization were investigated for long-term storage of the coated tubes. Then, the stability and accuracy of the kit in each method were compared. Test was done on 30 real samples in order to assess the accuracy of the produced kit under optimal conditions. The alignment of the results of the domestic and foreign kits’ accuracy was confirmed, which indicates lack of interference of the coated antibody with other blood serum components. Short-term precision of the kit was evaluated and SD <0.25 of the allowable total error (TEa=10%) was obtained within a run (Sw-run) for three control concentrations (low, medium, high). The long-term precision of the kit was also evaluated and S total<0.33 of the allowable total error (TEa=10%) was obtained in three runs for three control concentrations (low, medium, high).

CONCLUSION
Considering the results obtained, the kit’s quality control, calculated short-term and long-term imprecision according to accredited criteria of CLIA for diagnostic kits, the domestic kit produced without preliminary preparation has acceptable precision and suitable quality for measurement of PSA levels in serum.

ACKNOWLEDGMENTS
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CONFLICT OF INTEREST
We have no conflict of interest to declare.

REFERENCES


